Bio-inspired algorithms based on sparse representations of signals for apnea-hypopnea events detection

> Ing. Román E. Rolón Director: Dr. Hugo L. Rufiner Co-Director: Dr. Rubén D. Spies

IMAL seminar

June 2, 2017







2 Motivation

3 Related works

Sparse representations of signals

6 Proposal

- Discriminative methods for signal classification
- Measuring complexity in sparse representations
- Multi-class discriminative dictionary learning

6 Conclusions

Image: A mathematical states and a mathem

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The main objective of this research is the development, use and evaluation of advanced biomedical signal processing techniques and machine learning algorithms for identifying pathologies associated to sleep disorders.

Specifics

- Develop methods based on sparse representations of pulse oximetry signals by using optimization techniques and inverse problems for the detection of obstructive sleep apnea-hypopnea syndrome.
- Include discriminative information to sparse representations for biomedical signals classification.
- Use of databases with real studies for applying and validating the proposed methods.
- Compare the proposed method with those well-know traditional ones.
- Analyze and validate the results.

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Obstructive Sleep Apnea-Hypopnea Syndrome (OSAHS)

OSAHS is one of the most common sleep disorders, which is caused by repeated events of partial (hypopnea) or total (apnea) obstruction of the upper airway while sleeping.

OSAHS illustration



(a) Normal

(b) Partial obstruction

(c) Total obstruction

Image: A math a math

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- Is a highly prevalent syndrome in the general human population.
- Affects up to 5 % of men and 3 % of women.
- The diagnosing method is normally very limited as well as costly in terms of both time and money.
- Aging, being male, snoring and obesity are all factors increasing the risk of suffering this pathology.
- Sleep fragmentation, intermittent hypoxemia, increased sympathetic tone and hypertension are main causes of mortality and morbidity.
- There is evidence that close to 93% of women and 82% of men with moderate to severe OSAHS remain undiagnosed.

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- Apnea event: Cessation of airflow at least 10 seconds.
- Hypopnea event: Reduction of airflow accompanied by a desaturation of at least 4%.
- Desaturation: Blood oxygen reduction.
- Apnea-hypopnea index (AHI): Represents the average number of apnea-hypopnea events per hour of sleep.

OSAHS severity

- Healthy if $AHI \in [0, 5)$.
- Mild if $AHI \in [5, 15)$.
- Moderate if $AHI \in [15, 30)$
- Severe if $AHI \in [30, \infty)$.

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Nocturnal polysomnography (PSG)



Importance of simplified studies!

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Nocturnal polysomnography (PSG)



Importance of simplified studies!

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Biomedical signals coming from a polysomnography



It is possible to detect the apnea-hypopnea events by "analyzing" only the pulse oximetry signal?

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Biomedical signals coming from a polysomnography



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Hypothesis 1

It is really possible to detect OSAHS using only the pulse oximetry signal.

Pulse oximetry



Hypothesis 2

The inclusion of *discriminative information* in the sparse representation of pulse oximetry signals allows for improving the performance and providing robustness in the detection of OSAHS.

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- J. Vázquez *et. al.*, Automated analysis of digital oximetry in the diagnosis of obstructive sleep apnoea, (2000).
- A. Yadollahi *et. al.*, Sleep apnea monitoring and diagnosis based on pulse oximetry and tracheal sound signals, (2010).
- P. Laguna *et. al.*, Selection of nonstationary dynamic features for obstructive sleep apnoea detection in children (2011).
- G. Schlotthauer *et. al.*, Screening of obstructive sleep apnea with empirical mode decomposition of pulse oximetry, (2014).
- D. Alvarez-Estevez *et. al.*, Computer-Assisted Diagnosis of the Sleep Apnea-Hypopnea Syndrome: A Review, (2015).
- L. Hang *et. al*, Validation of overnight oximetry to diagnose patients with moderate to severe obstructive sleep apnea, (2015).
- A. Hassan, Computer-aided obstructive sleep apnea detection using normal inverse gaussian parameters and adaptive boosting, (2016).
- H. Karamanli *et. al.*, A prediction model based on artificial neural networks for the diagnosis of obstructive sleep apnea, (2015).

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Sparse re	presentatio	ons			

Problem statement

Let $X \doteq [\mathbf{x}_1 \ \mathbf{x}_2 \ \cdots \ \mathbf{x}_n] \in \mathbb{R}^{N \times n}$ a matrix composed by "*n*" *N*-dimensional signals, let $\Phi \doteq [\phi_1 \ \phi_2 \ \cdots \ \phi_M] \in \mathbb{R}^{N \times M} (M \gg N)$ a matrix (dictionary) whose columns (atoms) normalized via l_2 -norm. The problem can be written as $\mathbf{x} = \Phi \mathbf{a}$; where $(P_0) \quad \mathbf{a} = \operatorname{argmin} ||\mathbf{a}||_0$ subject to $\mathbf{x} = \Phi \mathbf{a}$, (1)

where $||\mathbf{a}||_0$ denotes the l_0 pseudo-norm of \mathbf{a} .

Convex relaxation

$$(P_1) \qquad \mathbf{a} = \operatorname*{argmin}_{\mathbf{a}} ||\mathbf{a}||_1 \text{ subject to } \mathbf{x} = \Phi \mathbf{a}, \tag{P}$$

where $||\mathbf{a}||_1$ denotes the l_1 norm of \mathbf{a} .

- Basis pursuit (BP). Chen et. al. (1999).
- Matching pursuit (MP). Mallat et. al. (1993).
- Orthogonal matching pursuit (OMP). Tropp et. al. (2007).
- Many others...

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Convex relaxation

$$(P_1) \qquad \mathbf{a} = \operatorname{argmin}_{\mathbf{a}} ||\mathbf{a}||_1 \text{ subject to } \mathbf{x} = \Phi \mathbf{a},$$

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where $||\mathbf{a}||_1$ denotes the l_1 norm of \mathbf{a} .

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Noise degree in the representation

$$P_2) \qquad \mathbf{a} \doteq \underset{\mathbf{a}}{\operatorname{argmin}} ||\mathbf{x} - \Phi \mathbf{a}||_2^2 \text{ subject to } ||\mathbf{a}||_1 \le p_0.$$
(3)

Dictionary learning

$$\langle \Phi, \mathbf{a} \rangle \doteq \underset{\Phi, \mathbf{a}}{\operatorname{argmin}} ||\mathbf{x} - \Phi \mathbf{a}||_2^2 + \lambda ||\mathbf{a}||_1,$$

where λ is a regularization parameter.

- Method of optimal directions (MOD). Engan et. al. (1999).
- Noise overcomplete ICA (NOCICA). Lewiki et. al. (1999).
- K singular value decompositions (KSVD). Elad et. al. (2004).
- Others.

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Image: A matrix and a matrix

 $s_{1}nc(i)$

Problem

- Detection of apnea-hypopnea events (binary classification).
 - Class 1 (C_1): Segments of SaO₂ signals with apnea event.
 - Class 2 (C_2): Segments of SaO₂ signals without apnea event.
- Database with 995 complete studies a .

 $^{a} \rm http://cci.case.edu/serc/$

$\operatorname{Polysomnography}$

- Airflow.
- Respiratory effort.
- Electrical activity of the brain along the scalp.
- Electrical activity of the heart using electrodes placed on the body's surface.
- Electrical activity produced by skeletal muscles.
- Blood oxygen saturation.
- Others.
- Annotations of sleep stages, arousals and apnea-hypopnea events.

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Block diagram of the proposed system





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(d) Scaling function ϕ . (e) Wavelet function ψ

Main properties: asymmetric, orthogonal and biorthogonal.

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Right! Wavelet Daubechies 2



Main properties: asymmetric, orthogonal and biorthogonal.



The signal matrix is defined as:

$$X \doteq \left[\mathbf{x}_1 \ \mathbf{x}_2 \ \mathbf{x}_3 \ \mathbf{x}_4 \ \mathbf{x}_5 \cdots \mathbf{x}_{n-4} \ \mathbf{x}_{n-3} \ \mathbf{x}_{n-2} \ \mathbf{x}_{n-1} \ \mathbf{x}_n\right].$$
(5)

$$\sum_{x_{n-1}} \sum_{x_{n-1}} \frac{x_{n-1}}{x_{n-1}} \cdots \frac{x_{n-1}}{x_{n-1}}$$

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Let $\eta_1^j \doteq p(a_j \neq 0 | \mathbf{x} \in C_1)$ and $\eta_2^j \doteq p(a_j \neq 0 | \mathbf{x} \in C_2)$ being the probabilities of activation of the jth-atom for data belonging to the classes k = 1 and k = 2,

respectively. The discriminative measure for atoms selection is as follow:

$$D\{\eta_1^j, \eta_2^j\} \doteq |\eta_1^j - \eta_2^j|.$$
(6)

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Simplified steps of the proposed system

Given X and p_0 :

- Learn Φ by using NOCICA method.
- Obtain sparse codes \mathbf{a}_i by applying OMP algorithm.
- Apply Eq. (6) for detecting the most discriminative atoms (ϕ_d) of Φ .
- Construct a sub-dictionary $\hat{\Phi}$ by using ϕ_d .
- Obtain the new sparse codes \mathbf{a}_i by applying OMP algorithm.
- Train a MLP neural network for data classification.
- Test the performance of the system using the testing database.

Return AHIest

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 Conclusions

Experimental setup

- The complete dataset contains 995 studies, 41 of which were discarded due to incomplete information.
- $\bullet\,$ Among the remaining 954 studies, a subset of 667 (70 %) studies were randomly selected and fixed for training.
- $\bullet\,$ The final test was made using the remaining 287 $(30\,\%)$ studies of the database.
- The NOCICA method was used for the dictionary learning stage.
- Sparsity level $p_0 = 16$ was chosen.
- $\bullet\,$ The representation coefficients ${\bf a}$ were obtained by applying the OMP algorithm.
- A variation of the back-propagation algorithm, called mini-batch training procedure, was used to train the MLP neural network.

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Most discriminative atoms of the dictionary



creasing order of magnitude.

(j) $D \doteq |\eta_1^j - \eta_2^j|$ ordered in de- (k) Waveforms of the atoms corresponding to three different regions of D.

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 $\frac{s_{10}(i)}{s_{10}(i)}$

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Discrimin Results	native metl	hods for signal	l class	ification	
Performan	ce measures				
• Sensit	tivity:				
		SE	$= \frac{1}{VP}$	$\frac{VP}{P+FN}$.	(7)
 Specif 	ficity:			1 7 1 7	
		SP	$V = \frac{1}{VN}$	$\frac{VN}{V+FP}$.	(8)
• Accur	acy:		V	$P \perp VN$	

$$ACC = \frac{VP + VN}{P + N}.$$
(9)

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• Area under de ROC curve.

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A comparison of the performance measures obtained for the detection of OSAHS using different methods

Method	$\mathrm{AHI}_{\mathrm{thr}}$	AUC	SE(%)	SP(%)	ACC(%)
Proposed	10	0.906	81.40	79.31	80.35
	15	0.937	85.65	85.92	85.78
Chiner <i>et al.</i>	10	0.810	77.87	76.00	76.93
	15	0.795	76.17	78.12	77.15
Vázquez et al.	10	0.870	77.47	84.00	80.74
	15	0.909	80.84	87.50	84.17
Schlotthauer <i>et al.</i>	10	0.890	80.63	84.00	82.32
	15	0.922	84.11	85.94	85.02

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ROC curve analysis



 $\frac{s_{10}(i)}{s_{10}(i)}$



Final feature vectors to apnea-hypopnea events correlation¹



Are the hypotheses verified?

¹R. Rolón, L. Larrateguy, L. Di Persia, R. Spies and L. Rufiner, Discriminative methods based on sparse representations of pulse oximetry signals for sleep apnea-hypopnea detection. *Biomedical Signal Processing and Control (BSPC)*, Nol. 33, (2017), pp. 358-367.

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Block diagram of the proposed system



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Measurin Complexity	$g \ complex$	ity in sparse i	repres	entations	

Absolute difference of frequency activation

$$l_R\{\eta_1^j, \eta_2^j\} \doteq |\eta_1^j - \eta_2^j|.$$
(10)

Kullback-Leibler (KL) divergence

$$d_{KL}\{\eta_1||\eta_2\} \doteq \sum_{j \in M} \eta_1^j \log \left(\frac{\eta_1^j}{\eta_2^j}\right),\tag{11}$$

under the assumption that $0 \log(0) \doteq 0$.

J-divergence

$$d_J\{\eta_1, \eta_2\} \doteq d_{KL}\{\eta_1 || \eta_2\} + d_{KL}\{\eta_2 || \eta_1\}.$$
(12)

Jensen-Shannon divergence

$$d_{JS}\{\eta_1,\eta_2\} \doteq \frac{1}{2} d_{KL}\{\eta_1 || \eta_3\} + \frac{1}{2} d_{KL}\{\eta_2 || \eta_3\},\tag{13}$$

where $\eta_3 = \frac{\eta_1 + \eta_2}{2}$.

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Measurin	ng complex	ity in sparse :	repres	entations	



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Images representing performance measures obtained by different percentages of sparsity and different dictionary sizes





 $(\mathbf{o}) \Phi_J$.



 $(\tilde{n}) \Phi_{KL}$.



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Proposal

Development of a discriminative dictionary learning algorithm for multi-class signal classification using a generalized version of the absolute difference of frequency activation measure.

Discriminative coupled dictionary

The dictionary $\Phi \in \mathbb{R}^{M \times \kappa}$ is composed by a collection of sub-dictionaries $(\Phi_{c\kappa})$ as follows:

$$\Phi = [\Phi_{c1} \ \Phi_{c2} \ \cdots \ \Phi_{c\kappa}], \text{ (para } \kappa \text{ clases)}$$
(14)

where $\Phi_{c\kappa} = [\phi_{c\kappa}^1 \ \phi_{c\kappa}^2 \ \cdots \ \phi_{c\kappa}^I]$, (*I* distribution atoms for each class)

Discriminative measure

$$D(j,k) = \eta_k^j - \max_{\kappa \neq k} \left(\eta_\kappa^j \right).$$
(15)

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Multi-class discriminative dictionary learning



Image: A matrix and a matrix

Proposal Multi-class discriminative dictionary learning Proposed algorithm Algorithm 1 DKSVD 1: procedure DKSVD (X, p_0, r, I, κ) inc = 1for $i \leftarrow 1, I$ do $\Phi_{init} \leftarrow \text{Ksvd}(X, p_0)$ Get sparse matrix $A = [A_1 \ A_2 \ A_3 \ \cdots \ A_n]$ that accomplish $X = \Phi A$ Get D according to Ec. (4) 6; Get Φ_d and Rem if $Rem = \emptyset$ then 9 inc = 0end if 10: while inc = 1 do 11: Get \hat{X} by removing the input signals corresponding to the discriminative atoms 12: $\Phi \leftarrow \text{Ksvd}(\hat{X}, p_0)$ 1.3 Get sparse matrix A that accomplish $\hat{X} = \Phi A$ 14: Get D according to Ec. (15) 15: 16:Get Φ_d and Remif $Rem = \emptyset$ then 17: inc = 018 end if 19: 20: end while $\Phi_D \leftarrow [\Phi_D \ \Phi_d]$ 21:Remove signals. 22: end for 23: $\Phi_D \leftarrow [\Phi_{c1} \ \Phi_{c2} \ \cdots \ \Phi_{cn}]$ where $\Phi_{cn} = [\phi_{c1}^1 \ \phi_{c2}^2 \ \cdots \ \phi_{cn}^I]$ $s_{1}nc(i)$ 24: return Φ_D 25:26: end procedure

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Some atoms in a redundant dictionary learned using KSVD method



First six atoms for three of the classes captured by the proposed discriminative dictionary learning algorithm



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Publicatio	ons			

• R. Rolón, L. Di Persia, L. Rufiner and R. Spies, A method for discriminative dictionary learning with application to pattern recognition, VI Congreso de Matemática Aplicada, Computacional e Industrial (MACI), (2017).

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- Discriminative methods for signal classification
- Measuring complexity in sparse representations
- Multi-class discriminative dictionary learning

6 Conclusions

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Conclusions

- The sparse representations of pulse oximetry signals is undoubtedly a promising technique for the design of new methods for OSAHS detection.
- New discriminative methods based on sparse representations for signal classification were successfully applied for the detection of apnea-hypopnea events.
- It is possible to include discriminative information in the representation for improving the performance of the classifier.
- A quite good performance in the detection of OSAHS was obtained.

Image: A math a math

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Thanks!

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